Statistical virtual eye model based on wavefront aberration

Jie-Mei Wang^{1,2}, Chun-Ling Liu¹, Yi-Ning Luo², Yi-Guang Liu², Bing-Jie Hu^{1,2}

Foundation items: National Natural Science Foundation of China (No. 61173182, No. 61179071); Applied Basic Research Project (No. 2011JY0124) and International Cooperation and Exchange Project of Sichuan Province (No. 2012HH0004)

¹Department of Ophthalmology, West China Hospital, Sichuan University, Chengdu 610041, Sichuan Province, China

²Video and Image Processing Lab, School of Computer Science and Engineering, Sichuan University, Chengdu 610041, Sichuan Province, China

Correspondence to: Chun-Ling Liu. Department of Ophthalmology, West China Hospital, Sichuan University, Chengdu 610041, Sichuan Province, China chunlingsc@ 163.com; Yi-Guang Liu. Video and Image Processing Lab, School of Computer Science & Engineering, Sichuan University, Chengdu 610041, Sichuan Province, China lygpapers@yahoo.com.cn

Received: 2012-4-29 Accepted: 2012-9-18

Abstract

• Wavefront aberration affects the quality of retinal image directly. This paper reviews the representation and reconstruction of wavefront aberration, as well as the construction of virtual eye model based on Zernike polynomial coefficients. In addition, the promising prospect of virtual eye model is emphasized.

 KEYWORDS: wavefront aberration; wavefront reconstruction; virtual eve; Zernike polynomial

DOI:10.3980/j.issn.2222-3959.2012.05.15

Wang JM, Liu CL, Luo YN, Liu YG, Hu BJ. Statistical virtual eye model based on wavefront aberration. *Int J Ophthalmol* 2012;5 (5):620-624

INTRODUCTION

T he refractive system of human eye is mainly composed of cornea, lens, vitreous and others. However, just like other optical instruments, the human eye is not an ideal optical system. The difference of wavefront between the ideal optical system and the actual measured optical system is wavefront aberration ^[1]. Besides the mainly traditional low-order aberration ^[2], high-order aberration also exists in human eye. Low-order aberrations include tilts, defocus and astigmatism. While, other optical defects of refractive system, such as spherical aberration, coma, are included in high-order aberration. Refractive surgery can modify the human eye's optical system so as to improve the visual quality of the retina, which mostly corrects low-order aberrations such as myopia, hyperopia and astigmatism. It can improve the patients' evesight significantly, but some problems, such as poor night vision, glare monocular diplopia, which are mainly caused by high-order aberration, remain unsolved ^[3]. In order to improve the visual quality, it is necessary to further research the wavefront aberration. This paper reviews the representation and reconstruction of wavefront aberration, as well as methods of developing virtual eve from wavefront aberration. In addition, the promising prospect of virtual eye model is emphasized.

REPRESENTATION OF WAVEFRONT ABERRATION

The methods for representing wavefront aberration of human eye are as a list or a bar chart showing coefficients of normalized Zernike polynomials^[4], and in the form of a topographical map.

Coefficients of Zernike Polynomials Porter *et al* ^[5] found that Zernike polynomials can describe the wavefront aberration of human eye effectively in 2001. Smolek and Klyce *et al* ^[6] claimed that the higher of the order used in the Zernike polynomials, the greater of the fitting error will be. And Zernike method fails to capture all high-order aberration for eyes after corneal surgery which was concluded by Klyce^[7].

Typically, the ophthalmic coordinate system is used to describe the Zernike polynomials as shown in Figure 1. Zernike polynomials are orthogonal over the unit circle, so the coefficients are independent to each other ^[8]. The coefficients of Zernike polynomials can be formulated in double index or single index.

Double index representation The Zernike polynomials are usually presented as z_n^m (ρ , θ) in polar coordinate system, with the index *n* describing the order of the aberration and the index *m* representing the azimuthal frequency of the sinusoidal. The radius parameter is designed by the letter ρ

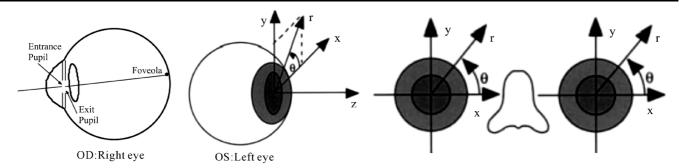


Figure 1 Ophthalmic coordinate system.

continuous over its range of 0 to 1.0, and θ means the azimuthal component continuous over its range of 0 to 2π . The wavefront aberration function W(x,y) can by presented as followings:

$$W(x,y) = \sum_{n,m} c_n^m z_n^m$$
(1)

$$z_n^m(\rho,\theta) = \begin{cases} N_n^m R_n^{[m]}(\rho) \cos m\theta & m > 0\\ -N_n^m R_n^{[m]}(\rho) \sin m\theta & m < 0 \end{cases}$$
(2)

$$R_{n}^{[m]}(\rho) = \sum_{s=0}^{(n-[m])/2} \frac{(-1)^{s}(n-s)!}{s![ns(n+|m|-s)]![0.5^{*}(n-|m|-s)]!} \rho^{n-2s}$$

$$N_{n}^{m} = \sqrt{\frac{2(n+1)}{1+\delta_{m,0}}} \quad \text{Or} \quad N_{n}^{m} = \sqrt{(2-\delta_{m,0})(n+1)}$$
(3)

Where, if m=0, $\delta_{m,0}=1$, otherwise, $\delta_{m,0}=0$.

Zernike polynomials are orthogonal in the sense that they satisfy the following equation:

$$\int_{0}^{\infty} \rho d_{\rho} \int_{0}^{2\Pi} z_{n}^{m} z_{n'}^{m'} d_{\theta} = \Pi \delta_{n,n'} \delta_{m,m'}, \qquad (4)$$

Where, if, n=n', $\delta_{n,n'}=1$, otherwise, $\delta_{n,n'}=0$

If, m=m', $\delta_{mm'}=1$, otherwise, $\delta_{mm'}=0$.

Single index representation In the above representation, the Zernike mode coefficient depends on two parameters, n and m. Occasionally, a standard single indexing scheme is more arbitrary for describing the coefficients of Zernike polynomials with the index j. While this scheme only be used for bar plots for the coefficients. Their relationships are as follows^[9]:

$$Z_{j} = Z_{n}^{m}$$

$$j = \frac{n(n+2) + m}{2}$$

$$n = \left[\frac{-3 + \sqrt{9 + 8j}}{2}\right]$$

$$m = 2j - n(n+2)$$
(5)

Topographical Map Wavefront aberration is normally given in form of series of polynomial coefficients, root mean square (RMS) values, 2D contour plots, 3D surface plots, or vergence map. The vergence map is the standard format for topographic representation of wavefront aberration of human eye, and it can be obtained from the wavefront senor directly, without the wavefront aberration

reconstruction^[10]. Map is convenient for doctors to catch the distribution of the patient's eye aberration with the intuitionistic representation provided by wavefront aberration diagram.

WAVEFRONT ABERRATION RECONSTRUCTION

The representation of wavefront aberration of human eye is introduced above. In general, aberrometry measures the slope of wavefront in the eye ^[10], and we can reconstruct the wavefront aberration of human eye using Zernike reconstruction algorithm by the slope ^[11,12]. Jeong *et al*^[13] reconstructed wavefront aberration by use of Zernike polynomials in 2007. The simulated wavefront data from corneal topography to calculate corneal aberration was obtained by Geunyong Yoon *et al*^[14], and they concluded that the Zernike method outperformed the Fourier method using the slop information.

The Theory of Wavefront Aberration Reconstruction In the wavefront aberration reconstruction, to posit and track the pupil automatically, the initial parameters should be set firstly and faculae image can be gained by Hartmann-Shark sensor. Then the centroid of every faculae was calculated as the actual focus of wavefront. Finally, coefficients of Zernike polynomials, which present wavefront aberration, are calculated by a series of formulas.

Centroid Localization The reconstruction of wavefront aberration based on the distance between standard center and actual center. So it is very important to select an accurate standard value, especially when the difference is very large ^[15-17]. Gravity method can be used to calculate the actual center in wavefront aberration reconstruction. We can calculate the centroid according to ^[11,14,18,19,20]:

$$x_{i} = \frac{\sum_{k}^{i} I_{ij} x_{ij}}{\sum_{k}^{m_{i}} I_{ij}} \qquad \qquad y_{i} = \frac{\sum_{k}^{i} I_{ij} y_{ij}}{\sum_{k}^{m_{i}} I_{ij}} \qquad \qquad (6)$$

Where $I_{i,j}$ represents the amplitude of the pixel in the sub-aperture, $x_{i,j}$ and $y_{i,j}$ are the coordinates of *j* th pixel in the *i* th sub-aperture, respectively.

Zernike polynomials are orthogonal over the unit circle in theory, and hence the discrete sampling data is required to be normalized before using Zernike polynomials for wavefront aberration reconstruction. (While there is a necessary normalize the discrete sampling data first.) These data is up to the center and the radius, the normalized coordinate can be obtained as follows: $x' = (x-x_0)/r_{0}$, $y' = (y-y_0)/r_0$. Where (x,y) is the initial coordinate, (x',y') means the normalized coordinate, the center coordinate is (x_0,y_0) , the symbol of r_0 represents the radius. And the error of (x_0,y_0) and r_0 will affect the accuracy.

The same size of pupil is absolutely necessary when comparing wavefront aberration, because the size of pupil will affect Zernike coefficients directly, Wang *et al*^[21] showed that the increase of pupil's diameter would not lead to all high order aberration increase correspondingly. Spherical aberration from 4mm to 5mm pupil size increased less than from 5mm to 6mm, and other high order aberration showed only a small increase with pupil dilation^[21].

Methods of Wavefront Aberration Reconstruction

Least Square Method In 2009, ANSI presented that Zernike coefficients can be generated based on the principle of least squares using the slope information of wavefront. This method is fitting the data to a set of polynomials $\{Z_j\}$, where j ranges from unity to the total number of polynomials^[22], and the polynomials are Zernike polynomials. Zc=G (7)

Where Z contains slope information for Zernike polynomials, the vector of Zernike coefficients is, every column of G can be obtained from wavefront aberrometer. The aim of reconstruction is to determine the values of the coefficients in the vector^c. The solution of least squares method is given by

$$c = [ZTZ]^{1}Z^{T}G$$
(8)

Where, Z^T is transpose of matrix Z, and $[Z^T Z]^{-1}$ is the inverse matrix of $Z^T Z$.

With, the final reconstruction of wavefront aberration is:

$$W(x, y) = \sum_{k=1}^{j} c_k z_k(x, y)$$
(9)

The method of calculating Zernike coefficients by Least Square Method is relatively stable in the case of noise, which is noted by J. Y. in 1980. He also showed that the result of Gram-Schmidt orthogonal transform method is competitive ^[23]. Besides, the equation is often seriously ill and contradictory when the data is larger with n>>j, where n is the number of rows of Z, and the exact solution can not be obtained. In 2006, Cao et al [24] obtained fitting coefficients by the way of making the contradiction equation Orthogonal triangular through Householder and transformation. The result showed that relative error of each order coefficient is less than $10\%^{[24]}$.

Gram – Schmidt Orthogonal Transformation Instead of using the in version method as least square method, which is numerically unstable, Gram-Schmidt Orthogonal Transformation method doesn't determine the Zernike coefficients directly. And the method seeks to generate an orthogonal set p from matrix.

$$G=pb$$
 (10)

Following the Gram-Schmidt orthogonal Transform procedure, the Zernike polynomials can be presented in terms of orthogonal sets P_k up to the order j; i.e.,

$$Z = [p_1, p_2, \dots, p_j] \begin{bmatrix} 1 & e_{12} & \dots & e_{1j} \\ 0 & 1 & \dots & e_{2j} \\ \vdots & \vdots & \ddots & \vdots \\ 0 & 0 & \dots & 1 \end{bmatrix}$$
(11)

The coefficients of Zernike polynomials are determined by the following relations:

$$\begin{bmatrix} b_1 \\ b_2 \\ \vdots \\ b_j \end{bmatrix} = \begin{bmatrix} 1 & e_{12} & \cdots & e_{1j} \\ 0 & 1 & \vdots & e_{2j} \\ \vdots & \vdots & \ddots & \vdots \\ 0 & 0 & \cdots & 1 \end{bmatrix} \begin{bmatrix} c_1 \\ c_2 \\ \vdots \\ c_j \end{bmatrix}$$
And then the expression of ^c is:
$$(12)$$

$$\begin{cases} c_{j} = b_{j} \\ c_{i} = b_{i} - \sum_{k=i+1}^{j} e_{ik}c_{k} \quad i = 1, 2, \cdots, j-1 \end{cases}$$
(13)

Gram-Schmidt Orthogonal Transformation improves the status of equation to a certain degree, but it still can not get rid of the construction of equation.

Householder Transformation The least square problem by Householder transformation is to make the coefficient matrix of orthogonal and triangular by Householder transformation.

$$Q \bullet Z = \begin{pmatrix} R \\ 0 \end{pmatrix}, \tag{14}$$

Where R represents upper triangular nonsingular real matrix with j order, 0 is zero matrix with n-j order, Q means orthogonal matrix with n order.

$$QgG = \begin{pmatrix} A \\ B \end{pmatrix},$$
 (15)

Where, A is j-dimensional column vector, B is n-j-dimensional column vector.

$$Q\delta = Q(G - Zc) = \begin{pmatrix} A \\ B \end{pmatrix} - \begin{pmatrix} R \\ 0 \end{pmatrix} c = \begin{pmatrix} A - Rc \\ B \end{pmatrix},$$
 (16)

Where, $\|\delta\|_2^2 = \|Q\delta\|_2^2 = \|A - Rc\|_2^2 + \|B\|_2^2$, *A-Rc* is vanished, $\|\delta\|_2^2$ will get the minimum and *Rc=A*, *c=R^{-1}A*.

Householder transformation is very stable since it can avoid the construction of equation. In 2009, Chen *et al*^[24] made a conclusion that the Householder transformation was better than Gram-Schmidt orthogonal transformation and Singular Value Decomposition by the standard of time-consuming and reconstruction precision. However, Gao *et al*^[12] thought this algorithm's calculation was too large in 2010.

Singular Value Decomposition (SVD) The Singular Value Decomposition algorithm is used to obtain generalized inverse of the coefficient matrix. The theory is simple and the calculation steps are few. Especially, it is

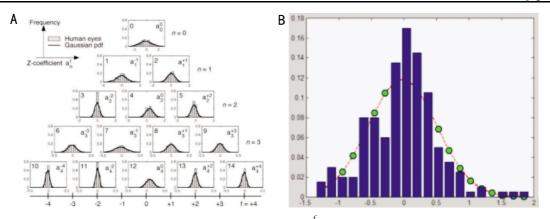


Figure 2 Frequency histogram of the Zernike polynomial coefficients a_n^{t} is the Zernike polynomial coefficients, *n* is the order, *f* is the frequency, the bar is frequency of the Zernike coefficients, the solid line is the Gauss fitting curve. The probability distribution of the Zernike coefficients in line was distributed with a Gaussian distribution as Figure 2B.

easy to program. In 2010, Gao *et al* ^[12] claimed that the singular value decomposition algorithm was the ideal wavefront aberration reconstruction algorithm. We can obtain wavefront aberration by wavefront aberration reconstruction based on the above methods.

VIRTUAL EYES

Physiological parameters (wavefront aberration) in the traditional model of the eye are fixed, but the wavefront aberration is individual. Virtual eye model with the individual aberration of wavefront is more close to real eyes. Recently, there exists two ways to generate virtual eyes, Gaussian model simulation and Monte Carlo simulation.

Gaussian Model Simulation As to functional virtual eyes based on Zernike coefficients, a group of Zernike coefficients could represent a virtual eye in Thibos's theory. According to the experimental results of the wavefront aberration, they confirmed that the coefficients of wavefront aberration polynomials are consistent with Gaussian model (Figure 2). They measure 100 optometry students in the age range 22-35 years and get 200 groups data from health eyes for a 6mm pupil.

Gaussian model generates 1000 groups random number (1000 group coefficients) by computer. In 2009, by the comparison of human eyes and statistical virtual eyes, it was claimed by them that the statistical virtual eyes slightly exaggerated the decline in retinal image quality ^[26-29].

For the population of normal eyes given in Thibos's study, each individual Zernike coefficient was reasonably well described as a random variable of Gaussian model, which has an appealing feature of simplicity. But for some abnormal eyes, this model is possibly inaccurate, it is necessary for us to verify it and find a more general and accurate model.

Monte Carlo Simulation In 2009, Li *et al* ^[30] obtained 20 groups Zernike coefficients and formed a 27×20 matrix. They got a group of Zernike coefficients as virtual eyes by

selecting one item from each row randomly. Based on this method, they got 100 virtual eyes by using Mat-lab.

The method of Monte Carlo simulation selected for generating virtual eyes is very simple and useful. Monte Carlo method is a random and reliable method in mathematics, but whether the wavefront aberration of human eye, which has its own characteristics, can be generated by that may be a little lack of theoretical basis.

APPLICATION PROSPECT OF VIRTUAL EYE

Wavefront aberration, presented by Zernike polynomials, has a wide range of applications in eye research and clinic ^[31]. While the researches between high order wavefront aberration and vision are still in primary stage.

We may quantify the quality of the retinal image by the point-spread function (PSF), optical transfer function (OTF), or the wavefront aberration function. The building of statistical virtual eyes makes it possible to simulate the influence of wavefront aberration to retinal image and to study individual variation in retinal image quality. Therefore, the establishment and application of statistical virtual eye model have a great deal of potential applications. One application of the model is to explore the human visual physiological mechanisms and computer vision theory; other potential applications are carrying out individual corneal refractive surgery, designing functional intraocular lens and corneal contact lens, evaluating of visual function, or exploiting ophthalmological apparatus and astronomical telescope with high image quality, and so on. Besides, that statistical virtual eye model is capable of generate large experimental reference data for various kinds of researches by computer. One advantage of this approach is that we can improve research efficiency by saving cost and time. Another advantage is that the model is generated as a stochastic process rather than a system with fixed parameters.

Researchers have made some works in the statistical virtual eye model. But, it is still a problem to make the statistical

Statistical virtual eye model

model of the virtual eye closer to the real eye. Simulate the eye in normal or various pathological states and assess the visual quality of different surgical approach or different intraocular lens implantation are unrealized, too. These problems still need a lot of hard works.

Acknowledgements: The authors thank Zeng-Xi Huang for critical comments and help with the paper revising.

REFERENCES

1 He JC, Burns SA, Marcos S. Monochromatic aberration in the accommodated human eye. *Vision Re*2000;40(1):41-48

2 Seiler T, Mrochen M, Kaemmerer M. Operative correction of ocular aberrations to improve visual acuity. *J Refract Surg* 2000;16(5):S619-622

3 Howlard HC. The history and methods of ophthalmic wavefront sensing. J Refract Surg2000;16(5):S552-553

4 Tang X, Zhu YX. Comparison of different wavefront aberrometers for measuring the wavefront aberrations of eyes with intraocular lenses. *Zhonghua Yanshiguang Xue Zazhr*2009;11(2):102–106

5 Porter J, Guirao A, Cox IG, Williams DR. Monochromatic aberrations of the human eye in a large population. *J Opt Soc Am A Opt Image Sci Vis* 2001;18(8):1793-1803

6 Smolek MK, Klyce SD. Zernike polynomial fitting fails to represent all visually significant corneal aberrations. *Invest Ophthalmol Vis Sci* 2003;44 (11):4676–4681

7 Klyce SD, Karon MD, Smolek MK. Advantages and disadvantages of the Zernike expansion for representing wave aberration of the normal and aberrated eye. *JRcfract Surg*2004;20(5):S537-541

8 Charman WN. Wavefront technology: Past, present and future. *Cont. Lens Anterior Eye*2005;28(2):75–92

9 Thibos LN, Applegate RA, Schwiegerling JT, Webb R; VSIA Standards Taskforce Members. Vision science and its applications. Standards for reporting the optical aberrations of eyes . *J Refract Surg.* 2002;18 (5): \$652-660

10 Iskander DR. Wavefront Modelling: Are the Zernike Polynomials the best Possible Approach? [EB/OL]. Wroclaw, Wroclaw University of Technology, 2010 [2012-01-01]. http://www.vog.if.pwr.wroc. pl/VOG/workshop/presentations/s1p1.pdf

11 Gao WW, Shen JX. Reconstruction technology wavefront aberration of human eye based on hartmann-shack senor. *Jiguang Shengwu Xuehao* 2010;19(3):408-412

12 Gao WW, Shen JX. Comparative study on algorithms for wave-front aberration reconstruction of human eye . *Guangpuxue yu Guangpu Fenxi* 2010;30(8):2232-2235

13 Jeong TM, Ko DK, Lee J. Method of reconstructing wavefront aberrations by use of Zernike polynomials in radial shearing interferometers. *Opt Lett* 2007;32(3):232-234

14 Yoon G, Pantanelli S, MacaRae S. Comparison of zernike and fourier wavefront reconstruction algorithms in representing corneal aberration of normal and abnormal eyes. *J Refract Surg* 2008;24(6):582–590

15 Davarinia F, Akhyani Z, Maghooli K. Total aberrations measurement with using the mathematical model of the eye. in Proceedings of the 2009 Third UKSim European Symposium On Computer Modeling and Simulation, 2009;169–174

16 Lundström L, Unsbo P, Gustafsson J. Off-axis wave front measurements for optical correction in eccentric viewing. *J Biomed Opt* 2005;10(3):034002

17 Thibos LN. Optical Models of the Eye [EB/OL]. 2012.1.1 http://www. opticsingobase.org/abstract.cfm?URI=FiO-2008-FThA1

18 Baik SH, Park SK, Kim CJ, Cha B. A center detection algorithm for Shack-Hartmann wavefront sensor. *Optic Laser Technol* 2007;39 (2): 262-267

19 Li HQ, Song HL, Rao CH, Rao XJ. Accuracy analysis of centroid calculated by a modified center detection algorithm for Shack-Hartmann wavefront sensor. *Optics Communications*2008;;281(4):750-755

20 Lu F, Wu JX, Qu J, Wang QM, Xu CC, Zhou XT, Shen YY, He JC. Association between offset of the pupil center from the corneal vertex and wavefront aberration. *J Optom* 2008;1(1):8–13

21 Wang Y, Zhao K, Jin Y, Niu Y, Zuo T. Changes of high order aberration with various pupil size in the myopic eye . *J Refract Surg* 2003;19 (2 Suppl): S270-274

22 ANSI Z80.28–2009. American National Standard for Ophthalmics: methods for reporting optical aberrations of eyes[S]

23 Wang JY, Silva DE. Wave-front interpretation with Zernike polynomials. *Applied Optics*1980;19(9):1510-1518

24 Cao ZL, Liao WH, Shen JX. A new algorithm for human eye's wave-front aberration fitting with Zernike polynomial. *Guangxue Jingmu Congeheug*2006;14(2):308-314

25 Chen ZY. Performance analysis of corneal aberration reconstruction with Zernike polynomials and slope. Master Thesis, Wenzhou Medical College, June 2009.

26 Thibos LN, Bradley A, Hong X. A statistical model of the aberration structure of normal, well-corrected eyes. *Ophthalmic Physiol Opt*2002;22 (5):427-433

27 Thibos LN, Hong X, Bradley A, Cheng X. Statistical variation of aberration structure and image quality in a normal population of healthy eyes. *J Opt Soc Am A Opt Image Sci Vis*2002;19(12):2329-2348

28 Thibos LN, Hong X, Bradley A, and Applegate RA. Accuracy and precision of objective refraction from wavefront aberrations. J Vis 2004;4 (4):329-351

29 Thibos LN. Retinal image quality for virtual eyes generated by a statistical model of ocular wavefront aberration. *Ophthalmic Physiol Opt* 2009;29(3):288-291

30 Li BY. Monte Carlo simulation of wavefront aberration. Master Thesis, Nankai University, June 2009.

31 Lundström L, Unsbo P. Unwrapping hartman-shack images from highly aberrated eyes using an iterative b-spline based extrapolation method. *Optom Vis Sci*2004;81(5):383-388